

# CT SCANNER PERFORMANCE EVALUATION

## **GREEN LIGHT IMAGING, LLC**

Medical Mobile Diagnostics  
8348 Rosemead Blvd  
Pico Rivera, CA 90660

(562)222-1321

**CDPH Facility ID: 78006**

### **CT Trailer #1**

GE BrightSpeed S  
Gantry S/N: 11905YC7

**Survey Date:** December 17, 2020

**Khachig A. Jerjian, Ph.D.**

ABR Certified in Diagnostic Radiological Physics  
California MQA-0061

(949)683-5215

## CT SCANNER PERFORMANCE EVALUATION SUMMARY

**Site:** GREEN LIGHT IMAGING, LLC  
 8348 Rosemead Blvd  
 Pico Rivera, CA 90660

**Report Date:** December 31, 2020  
**Survey Date:** December 17, 2020

**X-Ray Unit Manufacturer:** General Electric Medical Systems  
**Date Manufactured:** August 2007  
**Medical Physicist:** Khachig A. Jerjian, Ph.D.

**Model:** BrihtSpeed S  
**Room ID:** CT Trailer #1  
**Signature:**

### PASS/FAIL/NA

1. Review of Clinical CT Protocols	PASS
2. Scout Prescription Accuracy Evaluation	PASS
3. Laser Light Alignment Accuracy Evaluation	PASS
4. Table Travel Accuracy Evaluation	PASS
5. Radiation Beam Width Accuracy Evaluation	PASS
6. Slice Thickness Accuracy Evaluation	PASS
7. High Contrast Spatial Resolution Evaluation	PASS
8. Low Contrast Performance Evaluation	PASS
9. CT Number Accuracy Evaluation	
a. CT Number Accuracy and Linearity Evaluation	PASS
b. CT Number Contrast Scale Evaluation	PASS
c. CT Number Dependence on Slice Thickness Evaluation	PASS
d. CT Number Dependence on kVp Evaluation	PASS
e. CT Number and Image Uniformity Evaluation	PASS
10. Artifact Evaluation	PASS
11. Dosimetry Evaluation	PASS
12. Acquisition Display Device Evaluation	PASS
13. Radiation Protection Evaluation	
a. Visual Inspection	PASS
b. Audible/Visual Warning Signs	PASS
c. Posting Requirements	PASS
14. Technologist Quality Control Program Evaluation	PASS

## MEDICAL PHYSICS RECOMMENDATIONS & COMMENTS

1. CT scanner performance evaluation was found to be adequate. Performance evaluation test results were within ACR recommended action limits. Deviations in the indicated and measured  $CTDI_{vol}$  dose values were within an acceptable range of  $\pm 11\%$ .
2. Review of doses from representative clinical protocols were found to be adequate with typical doses well within ACR recommended Reference Dose Levels for both head and body protocols. Consider using a pitch factor of 1.375 instead of 1.75 with Adult Abdomen/Pelvis protocols.
3. Dosimetry spreadsheets and phantom images are attached for further details.
4. Detailed accounts of this performance evaluation may be obtained by contacting KJ Jerjian, Ph.D., at (949)683-5215.

**Khachig A. Jerjian, Ph.D., DABR**  
Medical Physicist

**Date: December 31, 2020**

## 1. REVIEW OF ROUTINE CLINICAL CT PROTOCOLS

This CT scanner performance evaluation was performed using the ACR CT Accreditation Program Phantom and routine clinical head and abdomen protocols used at this facility. Test procedures were consistent with ACR CT Accreditation Program guidelines.

**Table 1.** Routine Protocols

For this section, techniques used on an average patient or average technique calculated from several patient images is recorded.	<b>Adult Head</b>	<b>Adult Abdomen</b>	<b>Pediatric Head (1 Year Old)</b>	<b>Pediatric Abdomen (5 Year Old)</b>
kVp	120	120	120	120
mA	230	300	160	85
Time per Rotation (sec)	1.0	0.8	1.0	0.8
System Calculated mAs	230	240	160	100
Effective mAs (or mAs per slice) as displayed	245	137	119	73
Scan FOV (cm)	Head (25 cm)	Large (50 cm)	Ped (25 cm)	Large (50 cm)
Display FOV (cm)	25 cm	50 cm	25 cm	28 cm
Reconstruction Algorithm	Standard	Std Full	Std Plus	Std Plus
Axial (A) or Helical (H) Scan	H	H	H	H
Acquisition Slice Thickness Z-Axis Collimation (T in mm)	0.625	1.25	1.25	1.25
Number of Slices per Tube Rotation - # of Data Channels Used (N)	16	16	8	16
Table Increment (mm) (axial scans) or Table Speed (mm/rot)(helical scans) (I)	9.37	35.0	13.50	27.5
IEC definition of Pitch for this protocol (Pitch = I / N * T) (calculated by the System)	0.937	1.750	1.35	1.375
Reconstructed Scan Width (mm)	5.00	5.00	2.50	3.75
Reconstructed Scan Interval (mm)	5.00	5.00	2.50	3.75
Dose Reduction Technique(s) used in routine patient scanning for these protocols ( <i>Note: The ACR and CTDI phantoms are NOT scanned with dose reduction options.</i> )	Auto mA 100-200 mA Noise Index 2.69	Auto mA 100-300 mA Noise Index 10.44	Auto mA 50-170 mA Noise Index 5.44	Auto mA 50-200 mA Noise Index 12.35
Indicated CTDIvol (mGy)	54.99 mGy	12.33 mGy	23.80 mGy	4.40 mGy
Reference Dose Phantom Size	Head 16	Body 32	Head 16	Body 32

The facility clinical protocol acquisition and reconstruction parameters were reviewed for specific requirements of the diagnostic imaging task, adequate image quality and dose. The above listed protocols were found to be adequate. The High Resolution Chest protocol was also found to be adequate. Brain Perfusion protocols were not reviewed. Brain Perfusions are not performed on this scanner.

## 2. SCOUT PRESCRIPTION ACCURACY EVALUATION

**Phantom:** ACR CT Accreditation Phantom  
**Technique:** 120 kVp, 200 mA, 0.8 sec Rotation Speed, 160 mAs, Axial Mode, 2x0.625 mm Detector Configuration, 1.25 mm Slice Thickness, BonePlus Reconstruction Algorithm, Large SFOV, 21 cm DFOV, 512x512 Image Matrix.

Following proper position and leveling of the phantom on the scan table at the center of the gantry and acquisition of scout images, 1.25 mm thick axial images were prescribed at the center of modules 1 and 4 of the ACR CT Accreditation phantom at table landmark position of +0 mm and at table location 120 mm superior to the landmark position. Slice localization from scout prescription accuracy was evaluated using images of embedded 1 mm diameter BBs at the surface of modules 1 and 4 of the ACR phantom.

Detector Configuration	Nominal Position	Actual Location	Deviation (mm)
1i 2x0.625 mm	Landmark Location	0.0 mm	0.0 mm
	Superior +120 mm	+120.0 mm	0.0 mm

**Conclusion:** Slice localization from scanned projection radiographs/scout was found to be adequate, accurate to within  $\pm 1$  mm.

## 3. LASER LIGHT ALIGNMENT ACCURACY EVALUATION

Detector Configuration	Nominal Position	Actual Location	Deviation (mm)
1i 2x0.625 mm	Landmark Location	0.0 mm	0.0 mm
	Azimuth 0° Laser	Left/Right	0.0 mm
	Azimuth 90° & 270°	Vertical	0.0 mm

- Maximum discrepancy between the internal and external axial laser lights and the plane of radiation field was determined to be less than  $\pm 1$  mm. The sagittal and coronal laser light alignment accuracy was also found to be adequate, within  $\pm 2$  mm limits.

**Conclusion:** Bed positioning accuracy and congruence of the laser light beam localizer with the imaging plane was found to be adequate.

## 4. TABLE TRAVEL ACCURACY EVALUATION

Detector Configuration	Nominal Position	Actual Location	Deviation (mm)
1i 2x0.625 mm	Landmark Location	0.0 mm	0.0 mm
	Superior +120 mm	+120.0 mm	0.0 mm

- Maximum discrepancy in bed repositioning was determined to be less than  $\pm 1$  mm.

**Conclusion:** CT scanner table motion was accurate, reproducible and consistent with digital system indicators. Bed travel and indexing/incrementation accuracy was found to be adequate and reproducible to within  $\pm 1$  mm.

## 5. BEAM WIDTH ACCURACY EVALUATION

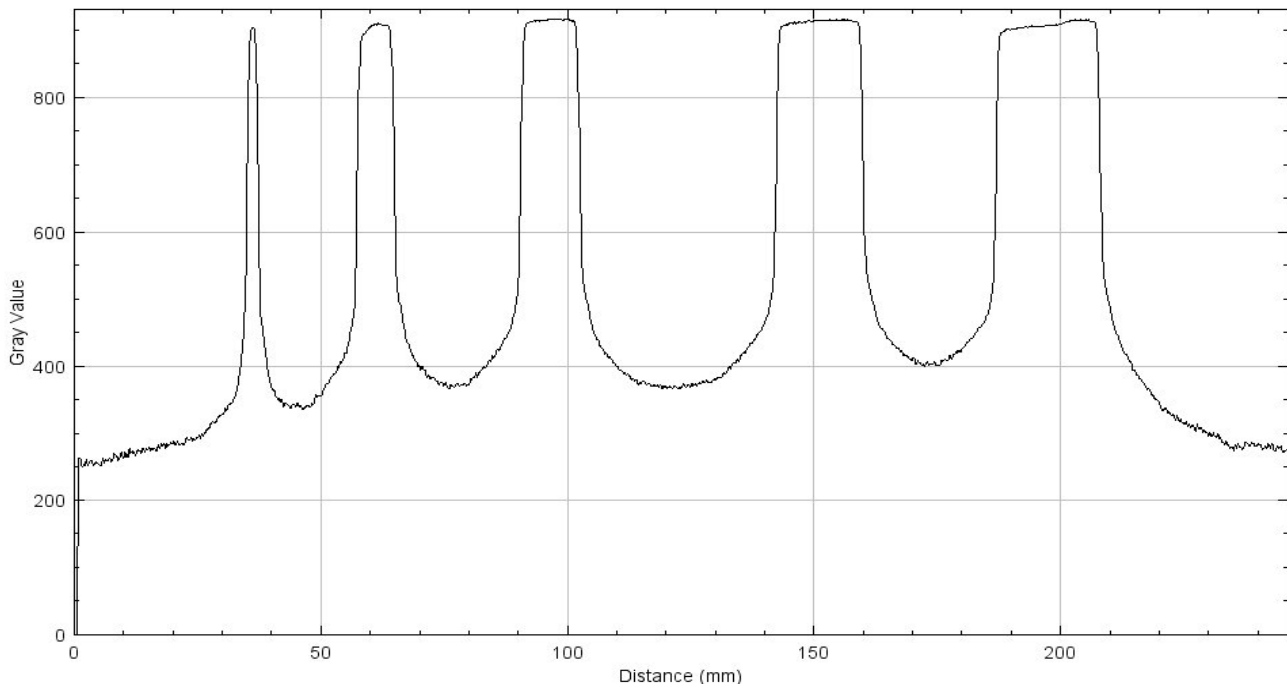
**Phantom:** CR Plate

**Technique:** 80 kVp, 10 mA, 0.8 sec Rotation Speed, 8 mAs, Axial Mode, Detector Configuration and Slice Thicknesses as indicated, Standard Reconstruction Algorithm, Large SFOV, 40 cm DFOV, 512x512 Image Matrix.

A CR plate was positioned at the iso-center and axial images were acquired at selected location. Beam widths were measured at the FWHM of the slice profiles.

Detector Configuration	Prescribed Beam Width	Measured Beam Width	Difference	STATUS
1i 2x0.625 mm	1.25 mm	2.7 mm	1.5 mm	PASS (< 3 mm)
1i 4x1.25 mm	5.0 mm	7.4 mm	2.4 mm	PASS (< 3 mm)
16i 16x0.625 mm	10 mm	12.2 mm	2.2 mm	PASS (< 3 mm)
4i 4x3.75 mm	15 mm	17.6 mm	2.6 mm	PASS (< 3 mm)
16i 16x1.25 mm	20 mm	21.4 mm	1.4 mm	PASS (< 6 mm)

**Conclusion:** Measured beam widths were found to be in good agreement with indicated beam widths. Measured beam widths have to be within the larger of  $\pm 3$  mm or 30% of prescribed total nominal collimated beam width.



## 6. SLICE THICKNESS ACCURACY EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1  
**Technique:** 120 kVp, 300 mA, 0.8 sec Rotation Speed, 240 mAs, Axial Mode, Detector Configuration and Slice Thicknesses as indicated, Standard Reconstruction Algorithm, Large SFOV, 21 cm DFOV, 512x512 Image Matrix.

Axial images were acquired at the center of Module 1 of the ACR CT Accreditation phantom. Slice widths were assessed by counting the visible wires on the two ramps containing wires arranged in 0.5 mm z-axis increments.

Detector Configuration (Prescribed Beam Width NxT)	Prescribed Slice Width	Measured Slice Width	Difference
16i 16x0.625 mm	0.625 mm	1.0 mm	< 0.5 mm
16i 16x1.25 mm	1.25 mm	1.5 mm	< 0.5 mm
8i 8x2.5 mm	2.50 mm	2.5 mm	0.0 mm
4i 4x3.75 mm	3.75 mm	4.0 mm	< 0.5 mm
4i 16x1.25 mm	5.0 mm	5.0 mm	0.0 mm
2i 4x3.75 mm	7.5 mm	7.5 mm	0.0 mm

**Conclusion:** Observed slice widths were found to be in good agreement with the nominal slice widths. Slice widths must be within  $\pm 1.5$  mm of the prescribed slice thickness.

## 7. HIGH CONTRAST SPATIAL RESOLUTION EVALUATION

**Phantom:** ACR CT Accreditation Phantom  
**Technique:** Routine Adult Head, Adult Abdomen and HR Chest Protocols

The high contrast resolution insert, Module 4 of the ACR Phantom, contains eight bar patterns representing spatial frequencies corresponding to 4, 5, 6, 7, 8, 9, 10 and 12 lp/cm, respectively.

Protocol	High Contrast Spatial Resolution
Routine Adult Brain Protocol	7 lp/cm
Routine Adult Abdomen protocol	7 lp/cm
HR Chest Protocol	10 lp/cm

**Conclusion:** The limiting high contrast spatial resolution is adequate. The ACR Pass/Fail criteria are 6 lp/cm for standard resolution head and body protocols and 8 lp/cm for the high resolution chest protocol.

## 8 (a). CONTRAST TO NOISE EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 2

**Technique:** Routine Head and Abdomen Protocols

The low contrast resolution insert, Module 2 of the ACR phantom, contains five different size rod sets with diameters equal to 6 mm, 5 mm, 4 mm, 3 mm, and 2 mm, respectively. The rod sets are considered to be resolved if all four rods of the same size can be clearly visualized .

### Contrast to Noise (CNR) Evaluation:

The low contrast resolution insert, Module 2 of the ACR Phantom, was evaluated using a ROI of about 100 mm<sup>2</sup>. Image noise was represented by the ROI standard deviation of the background area.

Protocol	Rod Insert ROI (H.U.)	Background ROI (H.U.)	Background ROI Std. Dev.	CNR
Adult Brain	94.1	88.2	4.6	1.3
Adult Abdomen	97.1	91.0	5.8	1.1
Pediatric Brain	95.0	87.9	8.6	0.8
Pediatric Abd	96.4	90.0	11.3	0.6

**Conclusion:** Routine Brain and Body protocol contrast to noise ratios were found to be adequate. The CNR must be greater than 1.0 for the adult Brain and adult Abdomen protocols. CNR must be greater than 0.7 for Pediatric Brain and greater than 0.4 for Pediatric Abdomen protocol.

## 8 (b). LOW CONTRAST RESOLUTION EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 2

**Technique:** Routine Adult Head and Adult Abdomen Protocols

The low contrast resolution insert, Module 2 of the ACR phantom, contains five different size rod sets with diameters equal to 6 mm, 5 mm, 4 mm, 3 mm, and 2 mm, respectively. The rod sets are considered to be resolved if all four rods of the same size can be clearly visualized .

Protocol	Contrast Level	CTDI <sub>vol</sub> (mGy)	Low Contrast Resolution
Adult Brain	0.6%	54.99 mGy	4 mm
Adult Abdomen	0.6%	12.33 mGy	4 mm
Pediatric Brain (1 Year old)	0.7%	23.80 mGy	5 mm
Pediatric Abdomen (5 Year old)	0.6%	4.40 mGy	6 mm

**Conclusion:** The ACR Pass/Fail criteria indicate a resolution of 6 mm diameter rods with both adult abdomen and adult brain protocols. The scanner Low Contrast Resolution is estimated to better than 4.0 mm @ 0.6 % contrast at a dose of 55 mGy CTDI<sub>vol</sub>.



## 9 (a). CT NUMBER ACCURACY AND LINEARITY EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1

**Technique:** Routine Brain and Abdomen Protocols

Module 1 of the ACR phantom is used to assess CT number accuracy and linearity. There are five cylinders of different materials including a bone mimicking material (“Bone”), polyethylene, water equivalent material, acrylic and air. Each cylinder, except the water cylinder, has a diameter of 25 mm and a depth of 4 cm. The water cylinder has a diameter of 50 mm and a depth of 4 cm. ROI measurements were performed in each insert with an ROI area of ~ 200 mm<sup>2</sup>.

**Technique:** Routine Adult Abdomen Protocol

ACR Phantom Insert	Mean CT Number (HU)	Acceptable CT Number Range
Polyethylene	-88	-107 HU to -84 HU
Water Equivalent	4.4	-7 HU to 7 HU
Acrylic	124	110 HU to 135 HU
Bone	899	850 HU to 970 HU
Air	<b>-962</b>	-1005 HU to -970 HU

**Technique:** Routine Adult Brain and Pediatric Brain and Abdomen Protocols

PROTOCOL	Adult Brain	Pediatric Brain	Pediatric Abdomen
Polyethylene Insert CT Number (HU)	-93	-92	-86
Water Equivalent Insert CT Number (HU)	1.4	2.6	5.3
Acrylic Insert CT Number (HU)	121	122	124
Bone Insert CT Number (HU)	<b>973</b>	<b>975</b>	898
Air CT Number (HU)	-982	-981	<b>-961</b>

**Conclusion:** CT number calibration accuracy is adequate. Mean CT numbers of tested inserts were mostly within ACR recommended ranges.

## 9 (b). CT NUMBER CONTRAST SCALE EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1

**Technique:** Routine Adult Brain and Adult Abdomen Protocols

CT number contrast scale was evaluated using the Water and Acrylic inserts in Module 1 of the ACR Phantom. Acrylic/Water CT number contrast scale was represented by the difference in Acrylic and Water CT numbers.

PROTOCOL	Acrylic CT Number	Water CT Number	Contrast Scale
Routine Adult Brain protocol	124	4	120 HU
Routine Adult Abdomen protocol	121	1	120 HU

**Conclusion:** Contrast scale is adequate. The acrylic and water CT number difference should be within 120 ± 12 HU.

### 9(c). CT NUMBER DEPENDENCE ON SLICE THICKNESS EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1  
**Technique:** Adult Abdomen equivalent axial protocol at 120 kVp, 300 mA, 0.8 sec Rotation Time, Large SFOV, 21 cm DFOV, Standard Body Algorithm, slice thicknesses as indicated and ROI areas of ~ 200 mm<sup>2</sup>.

Slice Thickness	Mean CT Number (HU)	Acceptable CT Number Range
0.625 mm	4.0	-7 HU to 7 HU
1.25 mm	3.6	-7 HU to 7 HU
2.5 mm	4.0	-7 HU to 7 HU
3.75 mm	3.2	-7 HU to 7 HU
5.0 mm	4.2	-7 HU to 7 HU
7.5 mm	3.4	-7 HU to 7 HU

**Conclusion:** CT number dependence on slice thickness is adequate. Mean CT numbers should be within the ACR recommended range of  $\pm 7$  HU, and preferably within  $\pm 5$  HU.

### 9(d). CT NUMBER DEPENDENCE ON kVp EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 1  
**Technique:** Routine Adult Abdomen equivalent protocol in axial mode 3.75 mm Slice Thickness, 250 mA and kVp values as indicated with ROI areas of ~ 200 mm<sup>2</sup>.

kVp	Mean CT Number (HU)	Acceptable CT Number Range
80	7.1	-7 HU to 7 HU
100	3.9	-7 HU to 7 HU
120	4.2	-7 HU to 7 HU
140	4.4	-7 HU to 7 HU

**Conclusion:** CT number dependence on kVp is adequate at 120 to 140 kVp, and borderline adequate at 80 kVp. Mean CT numbers should be within the ACR recommended range of  $\pm 7$  HU, and preferably within  $\pm 5$  HU.

## 9 (e). IMAGE UNIFORMITY EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 3

**Technique:** Routine Adult Abdomen Protocol

The uniformity section insert, Module 3 of the ACR phantom, contains Teflon beads embedded in a uniform water equivalent background. ROI measurements were performed at the center and periphery of the phantom. Area of ROI used was ~ 400 mm<sup>2</sup>. Image spatial uniformity was depicted by the edge-to-center mean CT number differences.

ACR Phantom	Location	Mean ROI CT Number (H.U.)	ROI Standard Deviation (H.U.)	Difference Center to Edge ROI (H.U.)
ROI ~ 400 mm <sup>2</sup>	Center	-0.2	6.2	---
	3 O'Clock	3.3		3.5
	6 O'Clock	2.6		2.8
	9 O'Clock	3.0		3.2
	12 O'Clock	3.6		3.8

**Conclusion:** Mean CT number and image spatial uniformity is adequate. The measured mean CT numbers should be in the range of  $0 \pm 7$  Hounsfield Units (HU) and preferably within  $0 \pm 5$  HU. Image spatial uniformity, depicted by the edge-to-center mean CT number differences is also within recommended limits. Edge-to-center mean CT number differences must be less than 5 HU for all four edge positions.

## 10. ARTIFACT EVALUATION

**Phantom:** ACR CT Accreditation and CTDI Dose Phantoms

**Technique:** Routine Adult Brain and Adult Abdomen Protocols

With all graphics turned off and with reduced room lighting, images were viewed for artifacts such as rings or streaks.

**Conclusion:** No significant ring, streak or other equipment related artifacts were noted.

## 11. CT DOSIMETRY EVALUATION

### A. CT SCANNER INDICATED COMPUTED TOMOGRAPHY DOSE INDEX (CTDI<sub>vol</sub>) EVALUATION

<b>Phantom:</b>	16 cm CTDI Acrylic Head and 32 cm CTDI Acrylic Body Phantom
<b>Dosimeter Used:</b>	Radcal Accu-Pro Model 9096 S/N 96-0544
<b>Ion Chamber:</b>	Radcal 10X6-3CT Ion Chamber
<b>Technique:</b>	Axial Brain and Abdomen Protocols

#### Weighted CTDI<sub>w,100</sub> Dose Measurements using CTDI Dose Phantoms:

Scan Protocols	kVp	mA	Scan Time (sec)	SFOV (cm)	Scan Type	Indicated CTDI <sub>vol</sub> (mGy)	Measured CTDI <sub>w</sub> (mGy)	Percent Difference
<b>Adult Brain</b> (16x0.625 mm)	120	230	1.0	Head (25 cm)	Axial	51.55 (Head16)	47.07	-9%
<b>Adult Abdomen</b> (16x1.25 mm)	120	300	0.8	Large (50 cm)	Axial	21.58 (Body32)	20.66	-4%
<b>Pediatric Brain</b> (16x0.625 mm)	120	160	1.0	Ped Head (25 cm)	Axial	32.13 (Head16)	28.47	-11%
<b>Pediatric Abdomen</b> (16x1.25 mm)	120	85	0.8	Large (50 cm)	Axial	6.05 (Body 32)	5.87	-3%

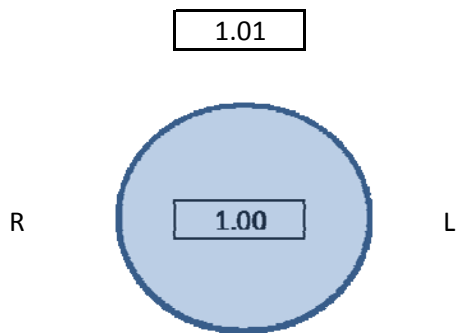
**CONCLUSION:** Measured CTDI<sub>w</sub> values were found to be consistent with indicated CTDI<sub>vol</sub> values. Percent differences were within an acceptable range of ± 10.0%.

#### RADIATION DOSE UNIFORMITY\*

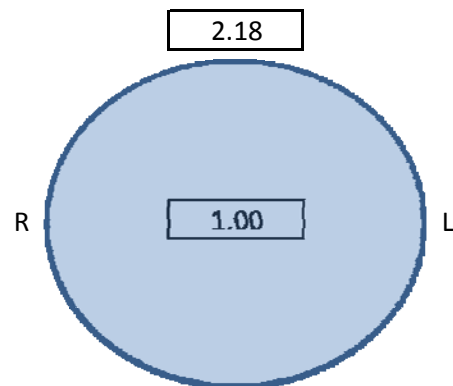
\*Note: Phantom surface dose factors normalized to the value at the center location

<b>Technique:</b>	120 kVp Adult Techniques as indicated in table above
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16 cm CTDI Head Dose Phantom



32 cm CTDI Body Dose Phantom



## 11. CT DOSIMETRY EVALUATION (Continued)

### B. PATIENT DOSE EVALUATION FOR REPRESENTATIVE CT EXAMINATIONS

**Phantom:** 16 cm CTDI Acrylic Head and 32 cm CTDI Acrylic Body Phantom

**Technique:** Routine Brain and Abdomen Protocols

**Correspondence of Measured and Indicated CTDI<sub>vol</sub> Doses for Select Clinical Protocols:**

Protocols	Measured CTDI <sub>vol</sub> (mGy)	Indicated CTDI <sub>vol</sub> (mGy)	Reference CTDI Dose Phantom	Percent Difference
Adult Brain	50.23 mGy	54.99 mGy	Head 16 cm	-9%
Adult Abdomen	11.81 mGy	12.33 mGy	Body 32 cm	-4%
Pediatric Brain	21.09 mGy	23.80 mGy	Head 16 cm	-11%
Pediatric Abdomen*	4.27 mGy	4.40 mGy	Body 32 cm	-3%

**CONCLUSION:** Measured CTDI<sub>vol</sub> dose values were found to be consistent with indicated CTDI<sub>vol</sub> values. Percent differences were within an acceptable range of  $\pm 10\%$ .

\*Note: Pediatric Abdomen dose measured using the Large (32 cm Diameter) CTDI Phantom.

### C. PATIENT DOSE EVALUATION FOR REPRESENTATIVE CT EXAMINATIONS

**Effective Dose Estimates for Select Clinical Protocols**

Protocols	Measured CTDI <sub>vol</sub> (mGy)	Scan Length	Dose Length Product DLP (mGy.cm)	Effective Dose (mSv)
Adult Brain	43.62 mGy	17.5 cm	763 mGy.cm	1.6 mSv
Adult Abdomen (SSDE)	12.10 mGy	25.0 cm	302 mGy.cm	4.5 mSv
Pediatric Brain	21.48 mGy	12.0 cm	258 mGy.cm	1.7 mSv
Ped Abdomen (SSDE)*	8.02 mGy	15.0 cm	120 mGy.cm	2.4 mSv

**CONCLUSION:** CTDI<sub>vol</sub> dose values and Effective Dose estimates are well within the ACR recommended limits. Attached, please find dose calculator spreadsheets for further details. Measured CTDI<sub>vol</sub> values should be less than the ACR Pass/Fail Criteria tabulated below, and preferably less than the ACR Reference Dose Levels.

**ACR CTDI<sub>vol</sub> Pass/Fail Criteria and CT Dose Reference Levels**

CT Examination	ACR Pass/Fail Criteria CTDI <sub>vol</sub> (mGy)	ACR Reference Levels CTDI <sub>vol</sub> (mGy)
Adult Head	80 mGy	75 mGy
Adult Abdomen	30 mGy	25 mGy
Pediatric Head (1 year old)	40 mGy	35 mGy
Pediatric Abdomen (40-50 lb) - 16 cm Diameter CTDI Phantom	20 mGy	15 mGy
Pediatric Abdomen (40-50 lb) - 32 cm Diameter CTDI Phantom	10 mGy	7.5 mGy

## 12 (a). ACQUISITION DISPLAY DEVICE EVALUATION

**Luminance Meter Make/Model:** Unfors Xi Photometer

**Acquisition display devices were evaluated using a standard SMPTE test pattern:**

1. The 5% and the 95% square contrast patterns were properly resolved and visualized.
2. Each gray-level step from 0% to 100% was uniform and distinct from the adjacent step.
3. The borders and lines of the SMPTE pattern were straight.
4. No spatial distortions or misalignments were noted in the grids across the screen.
5. Alphanumeric characters looked sharp and focused.
6. The high contrast line-pair resolution patterns in the center and corners of the display area were linear, properly resolved and adequately visualized without any magnification.
7. No streaking was noted in and around the white and black rectangular patterns.

The overall appearance of the SMPTE pattern was found to be adequate.

The soft copy display monitor resolution and spatial accuracy was found to be adequate.

No significant distortions or any kind of non-linearities were noted in any of the target patterns.

Monitor NEC MultiSync LCD 1980SXi	Minimum Luminance (Black Level)	Maximum Luminance (White Level)	% Luminance Non-Uniformity
Acquisition Workstation Display	0.5 cd/m <sup>2</sup>	142 cd/m <sup>2</sup>	15%

The minimum luminance (Black Level) should be less than 1.2 cd/m<sup>2</sup>.

The maximum luminance (White Level) should be greater than or equal 100 cd/m<sup>2</sup> for diagnostic workstations.

The display luminance uniformity is considered adequate if percent luminance non-uniformity is less than 30%.

**CONCLUSION:** The display monitor minimum & maximum luminances and uniformity were found to be adequate.

## 12 (b). SPATIAL DISTORTION EVALUATION

**Phantom:** ACR CT Accreditation Phantom Module 3

**Technique:** Routine Adult Abdomen Protocol

Spatial distortion and distance measurement accuracy was evaluated by measuring the known dimensions of the ACR phantom and set distance between the Teflon BB's in Module 3.

### A. Distance Gauge Check:

Orientation of BB's	Actual Distance Between BB's	Scanner Measured Distance	Percent Difference
45°	10.0 cm	10.0 cm	0.0%

### B. Aspect Ratio of Video Monitor and Imager (if available):

ACR Phantom	Aspect Ratio
Ratio of Horizontal to Vertical Dimensions of Circular Phantom Object	1.00
Ratio of Horizontal to Vertical Dimensions of Object on the Monitor	1.00
Ratio of Horizontal to Vertical Dimensions of Object on Film	N/A

**CONCLUSION:** The scanner distance measurement accuracy is adequate. There are no significant spatial distortion of the image on the monitors.

### 13. RADIATION SAFETY EVALUATION

A. Visual Inspection

A visual safety inspection of the CT Trailer and surroundings was conducted. No unsafe conditions were noted.

B. Audible and Visual Warning Signs

System audible and visual warning signs are functional and performing adequately. Dose Notification and Dose Alert features are activated and functioning properly.

C. Posting Requirements

CT scanner room was appropriately posted with a "Caution X-Ray" warning sign.

### 14. TECHNOLOGIST QUALITY CONTROL PROGRAM

A. Technologist QC program is well established. QC procedures are being properly performed and documented consistent with ACR CT Accreditation Program Guidelines.

Quality Control Procedures	Responsible Individual	Frequency	STATUS
1. Water CT Number Accuracy Eval	CT Technologist	Daily	PASS
2. Image Noise Evaluation	CT Technologist	Daily	PASS
3. Artifact Evaluation	CT Technologist	Daily	PASS
4. Visual Checklist	CT Technologist	Monthly	PASS
5. Dry Laser QC	CT Technologist	N/A	N/A
6. Acquisition Display QC	CT Technologist	Monthly	PASS

B. Preventive maintenance program is well established. Regular PMs are to be properly performed and documented by qualified field service engineers.

## ACR CT ACCREDITATION DOSE SPREADSHEET

IMPORTANT NOTE: This Excel Workbook contains formulae essential to accurate reporting of dose for ACR CT Accreditation. It is intended to be used with both Windows and Mac operating systems. Please note, ANY alteration of the formulae will very likely result in errors of reported data, and could adversely affect our accreditation results. You must enter accurate data from this workbook into the ACRedit online testing package. Please check the results from this workbook against the results shown in the ACRedit database online testing package before submission.

**Dose Calculator Spreadsheet (Exposure)**

**CTAP ID Number**

### Radiation Dosimetry (Adult Head)

CTDI Head Phantom (16-cm diameter PMMA Phantom)	Measured	Calculated
kV	120	
mA	230	
Exposure time per rotation (s)	1	
# data channels used (N) <sup>1</sup>	16	
Z-axis collimation (T) <sup>1</sup>	0.625	
Helical (H):Table Speed (mm/rot) = (I) <sup>1</sup>	9.37	
Active Chamber length (mm)	100	
Chamber correction factor	1	
<b>Center</b>		
Measurement 1 (mR)	533.7	
Measurement 2 (mR)	536.9	
Measurement 3 (mR)	534.7	
Average of above 3 measurements (mR)		535.1
Head CTDI at isocenter in phantom (mGy)		46.6
<b>12 o'clock position</b>		
Measurement 1 (mR)	542.1	
Measurement 2 (mR)	544.7	
Measurement 3 (mR)	544.9	
Average of above 3 measurements (mR)		543.9
Head CTDI at 12 o'clock position in phantom (mGy)		47.3
CTDI <sub>w</sub> (mGy)		47.07
<b>Clinical exam dose estimates (using measured CTDI<sub>w</sub> and site's Adult Head Protocol from Table 1)</b>		
CTDI <sub>vol</sub> (mGy)	=CTDI <sub>w</sub> *N*T/I	50.23
CTDI <sub>vol</sub> reported by scanner (mGy) for the protocol entered in the phantom site scanning data form (using 16-cm diameter PMMA phantom)	54.99	
Percent difference between calculated CTDI <sub>vol</sub> and CTDI <sub>vol</sub> reported by scanner		-9%
Dose Notification Value (mGy) as described in XR-29 (if applicable)		
DLP (mGy-cm)	=CTDI <sub>vol</sub> *17.5	879

<sup>1</sup>See definitions in the CT Accreditation Testing Instructions.

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## ACR CT ACCREDITATION DOSE SPREADSHEET

IMPORTANT NOTE: This Excel Workbook contains formulae essential to accurate reporting of dose for ACR CT Accreditation. It is intended to be used with both Windows and Mac operating systems. Please note, ANY alteration of the formulae will very likely result in errors of reported data, and could adversely affect our accreditation results. You must enter accurate data from this workbook into the ACRedit online testing package. Please check the results from this workbook against the results shown in the ACRedit database online testing package before submission.

### Dose Calculator Spreadsheet (Exposure)

CTAP ID Number

### Radiation Dosimetry (Adult Abdomen)

CTDI Body Phantom (32-cm diameter PMMA Phantom)	Measured	Calculated
kV	120	
mA	300	
Exposure time per rotation (s)	0.8	
# data channels used (N) <sup>1</sup>	16	
Z-axis collimation (T) <sup>1</sup>	1.25	
Helical (H):Table Speed (mm/rot) = (I) <sup>1</sup>	35	
Active Chamber length (mm)	100	
Chamber correction factor	1	
<b>Center</b>		
Measurement 1 (mR)	266.0	
Measurement 2 (mR)	267.3	
Measurement 3 (mR)	263.5	
Average of above 3 measurements (mR)		265.6
Body CTDI at isocenter in phantom (mGy)		11.6
<b>12 o'clock position</b>		
Measurement 1 (mR)	576.6	
Measurement 2 (mR)	579.0	
Measurement 3 (mR)	583.2	
Average of above 3 measurements (mR)		579.6
Body CTDI at 12 o'clock position in phantom (mGy)		25.2
CTDI <sub>w</sub> (mGy)		20.7
<b>Clinical exam dose estimates</b> (using measured CTDI <sub>w</sub> and site's Adult Abdomen Protocol from Table 1)		
CTDI <sub>vol</sub> (mGy)	=CTDI <sub>w</sub> *N*T/I	11.81
CTDI <sub>vol</sub> reported by scanner (mGy) for the protocol entered in the phantom site scanning data form (using 32-cm diameter PMMA phantom)	12.33	
Percent difference between calculated CTDI <sub>vol</sub> and CTDI <sub>vol</sub> reported by scanner		-4%
Dose Notification Value (mGy) as described in XR-29 (if applicable)		
DLP (mGy-cm)	=CTDI <sub>vol</sub> *25	295
SSDE for 35 cm water equivalent diameter (mGy)	=SSDE(35 cm)	12.10

<sup>1</sup>See definitions in the CT Accreditation Testing Instructions.

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### Dose Calculator Spreadsheet (Exposure)

CTAP ID Number

### Radiation Dosimetry (Pediatric Head, 1 year old)

CTDI Head Phantom (16-cm diameter PMMA Phantom)	Measured	Calculated
kV	120	
mA	160	
Exposure time per rotation (s)	1	
# data channels used (N) <sup>1</sup>	16	
Z-axis collimation (T) <sup>1</sup>	0.625	
Helical (H):Table Speed (mm/rot) = (I) <sup>1</sup>	13.5	
Active Chamber length (mm)	100	
Chamber correction factor	1	
<b>Center</b>		
Measurement 1 (mR)	312.0	
Measurement 2 (mR)	312.9	
Measurement 3 (mR)	311.6	
Average of above 3 measurements (mR)		312.2
Head CTDI at isocenter in phantom (mGy)		27.2
<b>12 o'clock position</b>		
Measurement 1 (mR)	332.9	
Measurement 2 (mR)	332.8	
Measurement 3 (mR)	338.4	
Average of above 3 measurements (mR)		334.7
Head CTDI at 12 o'clock position in phantom (mGy)		29.1
CTDI <sub>w</sub> (mGy)		28.47
<b>Clinical exam dose estimates</b> (using measured CTDI <sub>w</sub> and site's Pediatric Head (1 year old) Protocol from Table 1)		
CTDI <sub>vol</sub> (mGy)	=CTDI <sub>w</sub> *N*T/I	21.09
CTDI <sub>vol</sub> reported by scanner (mGy) for the protocol entered in the phantom site scanning data form (using 16-cm diameter PMMA phantom)	23.8	
Percent difference between calculated CTDI <sub>vol</sub> and CTDI <sub>vol</sub> reported by scanner		-11%
Dose Notification value as described in XR-29 (if applicable)		
DLP (mGy-cm)	=CTDI <sub>vol</sub> *12	253

<sup>1</sup>See definitions in the CT Accreditation Testing Instructions.

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## ACR CT ACCREDITATION DOSE SPREADSHEET

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### Dose Calculator Spreadsheet (Exposure)

CTAP ID Number

### Radiation Dosimetry (Pediatric Abdomen, 40-50 lb)

**Note: For pediatric abdomen (40-50 lb.) protocols, some CT scanners report CTDIvol using the 16 cm phantom, while others use the 32 cm phantom. The physicist should use the phantom (16 or 32 cm) that is used by the scanner to report CTDIvol.**

CTDI Phantom (16 or 32 cm diameter PMMA Phantom)	Measured	Calculated
Size of phantom the scanner uses to report CTDIvol for routine pediatric abdomen protocol (40-50 lb.)	<b>32 cm</b>	
kV	120	
mA	85	
Exposure time per rotation (s)	0.8	
# data channels used (N) <sup>1</sup>	16	
Z-axis collimation (T) <sup>1</sup>	1.25	
Helical (H):Table Speed (mm/rot) = (I) <sup>1</sup>	27.5	
Active Chamber length (mm)	100	
Chamber correction factor	1	
<b>Center</b>		
Measurement 1 (mR)	75.7	
Measurement 2 (mR)	76.0	
Measurement 3 (mR)	76.7	
Average of above 3 measurements (mR)		76.1
Ped Body CTDI at isocenter in phantom (mGy)		3.3
<b>12 o'clock position</b>		
Measurement 1 (mR)	164.5	
Measurement 2 (mR)	164.2	
Measurement 3 (mR)	164.7	
Average of above 3 measurements (mR)		164.5
Ped Body CTDI at 12 o'clock position in phantom (mGy)		7.2
CTDIw (mGy)		5.87
<b>Clinical exam dose estimates</b> (using measured CTDIw and site's Pediatric Abdomen (40-50 lb.) Protocol from Table 1)		
CTDIvol (mGy)	=CTDIw*N*T/I	4.27
CTDIvol reported by scanner (mGy) for the protocol entered in the phantom site scanning data form	4.40	
Percent difference between calculated CTDIvol and CTDIvol reported by scanner		-3%
Dose Notification Value as described in XR-29 (if applicable)		
DLP (mGy-cm)	=CTDIvol*15	64.1
SSDE for 18.5 cm water equivalent diameter (mGy)	=SSDE(18.5 cm)	8.02

<sup>1</sup>See definitions in the CT Accreditation Testing Instructions.

